



Factorial Optimization and Ex Vivo Evaluation of Cetirizine Microemulsions: Enhancing Transdermal Delivery via Combined Diffusion and Partitioning Mechanisms

Anayatollah Salimi ^{1,2}, Masoud Ali Karami ^{1,2}, Ehsan Afshari Hosseinpour ³, Yasaman Salimi ³, Hossein Heidari Kaydan ^{1,*}, Hamidreza Khalili ⁴, Amin Noori ⁵

¹ Department of Pharmaceutics, Faculty of Pharmacy, Ahvaz Jundishapur University of Medical Sciences, Ahvaz, Iran

² Nanotechnology Research Center, Ahvaz Jundishapur University of Medical Sciences, Ahvaz, Iran

³ Student Research Committee, Ahvaz Jundishapur University of Medical Sciences, Ahvaz, Iran

⁴ Department of Pharmacology, School of Pharmacy, Ahvaz Jundishapur University of Medical Sciences, Ahvaz, Iran

⁵ Traditional Medicine Clinical Trial Research Center, Shahed University, Tehran, Iran

*Corresponding Author: Department of Pharmaceutics, Faculty of Pharmacy, Ahvaz Jundishapur University of Medical Sciences, Ahvaz, Iran. Email: hkaydan1366@gmail.com

Received: 28 June, 2026; Revised: 16 July, 2026; Accepted: 21 July, 2026

Abstract

Background: Cetirizine is a zwitterionic, second-generation H₁-antihistamine widely used to treat allergic rhinitis and chronic urticaria. Although it has high oral bioavailability (> 70%), its use is limited by dose-related sedation and interindividual variability, supporting investigation of alternative topical and transdermal delivery approaches.

Objectives: This study aimed to formulate, optimize, and evaluate cetirizine microemulsions containing oleic acid and Transcutol P as natural-origin penetration enhancers, using a two-level full-factorial design, and to elucidate the mechanisms underlying enhanced ex vivo skin permeation.

Methods: Eight microemulsions were prepared using oleic acid and Transcutol P as the oil phase, Tween 80 and Span 20 as surfactants, and propylene glycol as a cosurfactant; each contained 1% (w/w) cetirizine. Oil content (5% and 50%), water content (5% and 10%), and the surfactant/cosurfactant ratio (1:1 and 3:1) were varied. The formulations were characterized for droplet size, polydispersity index, viscosity, pH, physical stability, in vitro release, and ex vivo rat-skin permeation. Factorial analysis was used to evaluate effects on steady-state flux (J_{ss}).

Results: Droplet sizes ranged from 14.94 to 46.15 nm, with a polydispersity index < 0.5. The optimal formulation, ME-CET-6 (5% oil, 10% water, S/C 1:1), yielded the highest flux (J_{ss} = 0.0431 ± 0.003 mg·cm⁻²·h⁻¹; ERflux = 5.42), representing an approximately 4.6-fold increase compared with the aqueous control. Factorial analysis identified oil content as the primary negative determinant of flux (P = 0.001), followed by the S/C ratio (P = 0.015), whereas water content was not significant (P = 0.119). Corrected diffusion enhancement ratios exceeded 1 for all microemulsions, indicating that improved diffusivity and partitioning jointly contributed to permeation enhancement.

Conclusions: Cetirizine microemulsions containing oleic acid and Transcutol P markedly enhance transdermal flux through combined increases in drug diffusivity and partitioning. These systems are promising candidates for further in vivo pharmacokinetic and skin irritation evaluation.

Keywords: Cetirizine, Microemulsion, Factorial Design, Permeability, Transdermal Delivery

1. Background

Cetirizine is a selective, second-generation histamine H₁-receptor antagonist with a rapid onset, a long

duration of action, and a low potential for interactions with drugs metabolized by hepatic cytochrome P450 (1, 2). It is used to treat allergic rhinitis and chronic urticaria and generally exhibits lower central nervous

Copyright © 2026, Salimi et al. This open-access article is available under the Creative Commons Attribution 4.0 (CC BY 4.0) International License (<https://creativecommons.org/licenses/by/4.0/>), which allows for unrestricted use, distribution, and reproduction in any medium, provided that the original work is properly cited.

How to Cite: Salimi A, Karami MA, Afshari Hosseinpour E, Salimi Y, Heidari Kaydan H, et al. Factorial Optimization and Ex Vivo Evaluation of Cetirizine Microemulsions: Enhancing Transdermal Delivery via Combined Diffusion and Partitioning Mechanisms. Jundishapur J Nat Pharm Prod. 2026;21(3):e173148. doi: <https://doi.org/10.5812/jjnpp-173148>

system penetration than first-generation antihistamines (3, 4).

Cetirizine is a zwitterion across the physiological pH range, with modest, constant octanol/water lipophilicity ($\log D \approx 1.5$ at pH 7.4) and a low volume of distribution (5, 6). Its oral bioavailability exceeds 70%, and its daily therapeutic dose is 5 - 10 mg (1, 2). However, sedation, interindividual variability, and the need for sustained symptom control support investigation of nonoral delivery approaches.

Transdermal delivery avoids first-pass metabolism and may improve convenience and compliance (11, 12). Efficient skin delivery requires an appropriate lipophilic-hydrophilic balance, a molecular weight generally below 500 Da, and sufficient thermodynamic activity in the vehicle (13). Microemulsions are thermodynamically stable, optically clear systems that can enhance skin delivery by increasing drug solubilization, modifying stratum corneum lipids, and improving drug partitioning into the skin (14-18).

Oleic acid and Transcutol P are widely used permeation enhancers. Oleic acid can disrupt lipid packing in the stratum corneum, whereas Transcutol P may increase drug solubility and partitioning (18-21). This research group has applied oleic acid/Transcutol P systems to celecoxib, vitamin B12, sildenafil citrate, methimazole, valproic acid, and doxepin (22, 25, 31-33), as well as to naproxen microemulsions (23) and to the liposomal and ocular delivery of curcumin, quercetin, and naringenin (24, 26, 34). Enhancer effects on cetirizine skin permeability, including those of oleic acid, Tween 80, and propylene glycol, have also been characterized by DSC and FTIR (10). Thus, the novelty of the present work lies not in the platform itself but in the factorial identification of the composition variables that control cetirizine flux and in the mechanistic interpretation of combined diffusion and partitioning enhancement.

2. Objectives

This study aimed to formulate and optimize cetirizine-loaded microemulsions based on oleic acid and Transcutol P; to evaluate their physicochemical properties, in vitro release, and ex vivo rat skin permeation; and to identify the formulation variables and transport mechanisms responsible for improved transdermal delivery.

3. Methods

3.1. Materials

Cetirizine was purchased from Abidi Pharmaceutical Company (Tehran, Iran). Transcutol P was supplied by Gattefosse (France). Tween 80, Span 20, propylene glycol, oleic acid, and monobasic and dibasic potassium phosphate were obtained from Merck (Germany). All solvents and reagents were of analytical grade.

3.2. Solubility Studies

The solubility of cetirizine in oils (oleic acid and Transcutol P), surfactants (Tween 80 and Span 20), and the cosurfactant (propylene glycol) was measured by adding excess drug to 2 mL of each solvent, stirring at 20 °C for 24 h, centrifuging, and analyzing the clear supernatant using a validated UV spectrophotometric method.

3.3. UV Method and Validation

Cetirizine was quantified by UV spectrophotometry. Standard solutions were prepared in methanol ($\lambda_{\max} = 238$ nm) and in water/0.1 N NaOH ($\lambda_{\max} = 230$ nm); the aqueous phosphate-buffer assay was performed at 230 nm. The method was validated for linearity, precision, accuracy, limit of detection, limit of quantification, and sink conditions (Table 1).

Table 1. UV Spectrophotometric Method Validation for Cetirizine (Aqueous Medium, 230 Nm)

Parameter	Value
Wavelength ($\lambda_{\max}$)	230 nm (aqueous); 238 nm (methanol)
Linearity range	2 - 20 $\mu\text{g}\cdot\text{mL}^{-1}$
Regression equation	$A = 0.0340C - 0.0294$
Coefficient of determination (R^2)	0.9993
Intra-day precision (%RSD)	1.67%
Inter-day precision (%RSD)	1.58%
Accuracy (% recovery)	99.8%
LOD	0.17 $\mu\text{g}\cdot\text{mL}^{-1}$
LOQ	0.50 $\mu\text{g}\cdot\text{mL}^{-1}$
Sink conditions	Confirmed (receptor <10% of saturation)

3.4. Animals

Male Wistar rats (10 - 12 weeks, 150 - 170 g) were obtained from the Central Animal House of Ahvaz Jundishapur University of Medical Sciences. Animals were housed in standard cages under a 12:12 h light/dark cycle, with ad libitum access to food and water. Abdominal skin was excised after anesthesia and euthanasia, cleaned of subcutaneous fat using cold acetone, and adjusted to a thickness of 250 ± 20 μm using a digital micrometer. Skin sections were randomly allocated to release and permeation experiments.

Table 2. Two-Level Full-Factorial Design of Cetirizine Microemulsions ^a

Formulation	Oil	Water	S/C ratio
ME-CET-1	50% (+)	10% (+)	3:1 (+)
ME-CET-2	50% (+)	10% (+)	1:1 (-)
ME-CET-3	50% (+)	5% (-)	3:1 (+)
ME-CET-4	50% (+)	5% (-)	1:1 (-)
ME-CET-5	5% (-)	10% (+)	3:1 (+)
ME-CET-6	5% (-)	10% (+)	1:1 (-)
ME-CET-7	5% (-)	5% (-)	3:1 (+)
ME-CET-8	5% (-)	5% (-)	1:1 (-)

^a Levels were coded as low (-) and high (+): oil 5% (-)/50% (+), water 5% (-)/10% (+), and S/C 1:1 (-)/3:1 (+). Cetirizine was fixed at 1% (w/w).

3.5. Experimental Design and Preparation

A two-level full-factorial design with three variables was used: oil content (5% and 50%), water content (5% and 10%), and S/C ratio (1:1 and 3:1), with cetirizine fixed at 1% (w/w), below its saturation solubility to maintain complete solubilization. The oil phase consisted of oleic acid/Transcutol P, the surfactant phase consisted of Tween 80/Span 20, and propylene glycol was used as the cosurfactant. The formulation design is shown in Table 2. Each formulation was prepared by dissolving cetirizine in the oil phase, mixing it with the surfactant-cosurfactant blend, and titrating with distilled water to form a clear microemulsion (23).

3.6. Characterization

Droplet size and polydispersity index (PDI) were measured using a particle-size analyzer (Scatter Scope 1 Quidex, South Korea), and the refractive index was measured using an Abbe refractometer. Viscosity was determined using a Brookfield DV-II+ Pro viscometer, and pH was measured at 25 °C.

3.7. Release and Skin Permeation

Release and permeation were evaluated using standing Franz cells (effective area, 4.906 cm²; receptor, 35 mL phosphate buffer, pH 7.4, 37 ± 0.5 °C, 200 rpm), yielding a skin-surface temperature of approximately 32 - 35 °C. For release, a cellulose membrane was placed between the donor and receptor compartments. For permeation, full-thickness abdominal rat skin was mounted with the stratum corneum facing the donor compartment. Samples were withdrawn at predetermined time points up to 24 h for release and up to 72 h for permeation, replaced with fresh receptor medium, and analyzed by UV spectrophotometry. Jss,

the permeability coefficient (P), lag time (T_{lag}), diffusion coefficient (D), and enhancement ratios (ER_{flux} = Jss,form/Jss,control; ER_D = D_{form}/D_{control}) were calculated from cumulative permeation profiles (23).

3.8. Physical and Chemical Stability

Physical stability was assessed at 4, 25, and 37 °C for 6 months by weekly inspection for transparency, phase separation, and changes in droplet size, and by centrifugation (10,000 rpm, 30 min). Chemical stability was assessed by measuring cetirizine content at 0, 3, and 6 months.

3.9. Statistical Analysis

Data are presented as mean ± SD (n = 3). Factor effects on Jss were analyzed using two-level full-factorial ANOVA (Minitab 17), including the three main effects and their interactions. Effect estimates, coefficients, and P values are reported, with P < 0.05 considered statistically significant.

4. Results

4.1. Solubility

Cetirizine solubility was highest in Tween 80 among the surfactants and in the oleic acid-Transcutol P combination among the oils (Table 3), supporting their selection. The 1% (w/w) load is below the aqueous saturation solubility and well below the solubility in the selected oil/surfactant mixture, thereby maintaining sink conditions in the dispersed phase and minimizing the risk of crystallization.

4.2. Factorial Design and Physicochemical Properties

Droplet sizes ranged from 14.94 to 46.15 nm, with PDI < 0.5, and were essentially unchanged after 6 months.

Table 3. Solubility of Cetirizine in Formulation Components (Mean $\pm$ SD, mg/mL, 20 °C)

Component	Role	Solubility (mg/mL)
Oleic acid	Oil phase	7.2 $\pm$ 0.1
Transcutol P	Oil phase	6.8 $\pm$ 0.2
Oleic acid + Transcutol P	Oil phase	11.9 $\pm$ 0.1
Span 20	Surfactant	9.5 $\pm$ 0.1
Tween 80	Surfactant	22.3 $\pm$ 0.2
Propylene glycol	Cosurfactant	19.3 $\pm$ 0.15
Water	-	10.0 $\pm$ 0.2

Table 4. Droplet Size, PDI, Size After 6 Months, Viscosity, and pH of Cetirizine Microemulsions (Mean $\pm$ SD)

Formulation	Size (nm)	PDI	Size 6 mo (nm)	Viscosity (cps)	pH
ME-CET-1	24.9 $\pm$ 1.25	0.39 $\pm$ 0.02	25.0 $\pm$ 0.5	376 $\pm$ 1.06	4.12 $\pm$ 0.01
ME-CET-2	14.94 $\pm$ 2.5	0.38 $\pm$ 0.01	15.8 $\pm$ 0.2	356 $\pm$ 1.04	4.43 $\pm$ 0.01
ME-CET-3	20.45 $\pm$ 2.2	0.39 $\pm$ 0.01	21.3 $\pm$ 0.1	604 $\pm$ 1.29	5.18 $\pm$ 0.02
ME-CET-4	46.15 $\pm$ 2.4	0.40 $\pm$ 0.02	47.10 $\pm$ 0.01	642 $\pm$ 1.21	5.13 $\pm$ 0.008
ME-CET-5	41.45 $\pm$ 1.3	0.41 $\pm$ 0.01	41.9 $\pm$ 0.5	320 $\pm$ 1.02	4.13 $\pm$ 0.03
ME-CET-6	26.95 $\pm$ 0.27	0.41 $\pm$ 0.01	26.98 $\pm$ 0.2	344 $\pm$ 1.11	4.30 $\pm$ 0.008
ME-CET-7	35.5 $\pm$ 1.1	0.40 $\pm$ 0.005	35.8 $\pm$ 0.1	235 $\pm$ 1.08	4.99 $\pm$ 0.02
ME-CET-8	18.95 $\pm$ 0.95	0.39 $\pm$ 0.01	19.5 $\pm$ 0.3	388 $\pm$ 1.16	5.55 $\pm$ 0.025

Viscosity ranged from 235 to 642 cps and increased with higher oil content and lower water content (both $P = 0.001$). pH ranged from 4.12 to 5.55 and was significantly affected by water content ($P = 0.008$) (Table 4).

4.3. Release

Release profiles over 24 h are shown in Figure 1, and release kinetics are summarized in Table 5. ME-CET-6 showed the highest 24-h release (72.21%), whereas ME-CET-3 showed the lowest release (51.19%). Release data were fitted to the zero-order, first-order, Higuchi, Korsmeyer-Peppas, and Log-Wagner models.

For ME-CET-6, the Korsmeyer-Peppas model yielded the highest adjusted r^2 (0.982); the modest first-order fit (0.877) indicates a non-first-order mechanism, consistent with diffusion/relaxation-coupled release.

4.4. Skin Permeation

Permeation parameters are shown in Table 6. All microemulsions increased flux relative to the control. ME-CET-6 provided the highest flux (0.0431 ± 0.003 mg·cm⁻²·h⁻¹) and permeability coefficient (0.051 ± 0.001 cm·h⁻¹), representing an approximately 4.6-fold increase over the control (0.0093 mg·cm⁻²·h⁻¹). The steady-state flux is shown in Figure 2.

Enhancement ratios are summarized in Table 7. Following re-examination, ERD was recomputed consistently as $D_{\text{formulation}}/D_{\text{control}}$ ($D_{\text{control}} = 0.0236$ cm²·h⁻¹). Corrected ERD exceeded 1 for all formulations (up to 7.44 for ME-CET-3), and ERflux reached 5.42 for ME-CET-6.

4.5. Effect of Formulation Variables on Flux

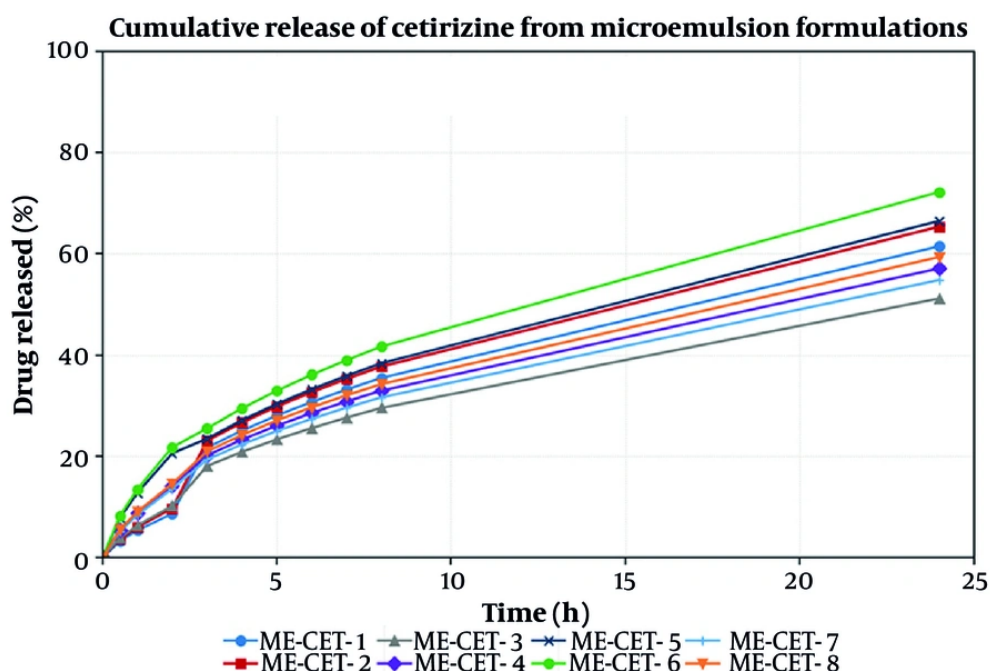
The factorial ANOVA of J_{ss} is shown in Table 8, with the fitted model $J_{ss} = 0.0340 - 0.000281(\text{oil}) + 0.000440(\text{water}) + 0.00185(\text{S/C})$. Oil content had the strongest significant effect ($P = 0.001$), followed by the S/C ratio ($P = 0.015$). Water content was not significant ($P = 0.119$). The main-effects plot is shown in Figure 3.

4.6. Comparison With Published Cetirizine Transdermal Systems

Table 9 compares the optimized formulation with published cetirizine skin-delivery systems. The most directly comparable study is the cetirizine nanoemulsion gel of Kassem et al., which also used a 2³ full-factorial design and rat-skin permeation and additionally included a clinical urticaria evaluation (36). That system reported a considerably higher permeability coefficient (7.65 cm·h⁻¹) than the present

Table 5. Best-Fit Release Kinetic Model, r^2 , and 24-H Cumulative Release (Q24) of Cetirizine Microemulsions

Formulation	Best-fit Model	r^2	Q24 (%)
ME-CET-1	Higuchi	0.9353	61.47
ME-CET-2	First-order	0.9547	65.36
ME-CET-3	First-order	0.9737	51.19
ME-CET-4	First-order	0.9718	57.11
ME-CET-5	First-order	0.9192	66.49
ME-CET-6	Korsmeyer-Peppas	0.9820	72.21
ME-CET-7	Log-Wagner	0.9740	54.83
ME-CET-8	Log-Wagner	0.9757	59.36

**Figure 1.** Cumulative release of cetirizine from microemulsion formulations over 24 h (mean $\pm$ SD, $n = 3$).

formulation ($0.051 \text{ cm} \cdot \text{h}^{-1}$); however, the two values are not directly comparable because of differences in dosage form, finite versus infinite dosing, receptor design, and reporting units. The present formulation provides a simpler microemulsion system with controlled factorial optimization and identifies the contributions of oil, water, and the S/C ratio to cetirizine flux.

4.7. Physical and Chemical Stability

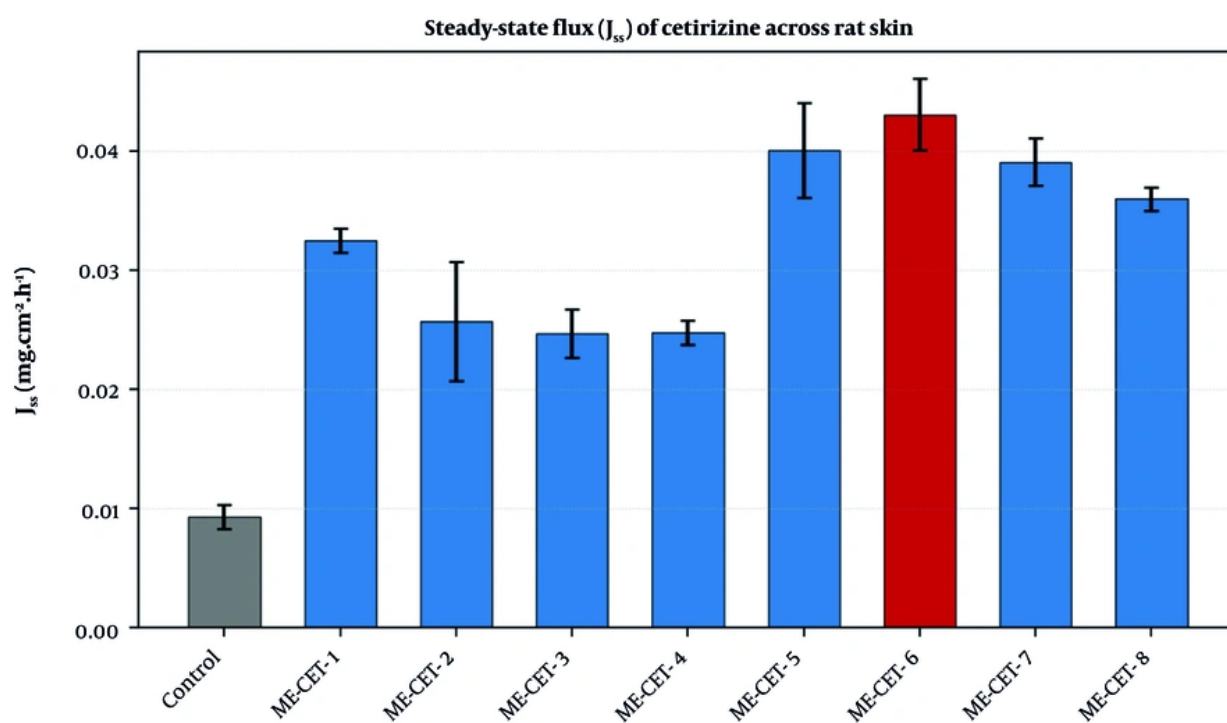
No turbidity, precipitation, or phase separation occurred over 6 months at 4, 25, and 37 °C, and none occurred after centrifugation (10,000 rpm, 30 min). Droplet size was essentially unchanged (Table 4). Cetirizine content after storage remained within the validated assay range, indicating the chemical stability of the selected microemulsions during the study period.

5. Discussion

Eight cetirizine microemulsions were prepared and evaluated using a two-level full-factorial design. Droplet

Table 6. Skin-Permeation Parameters of Cetirizine Microemulsions and Aqueous Control (Mean $\pm$ SD, N = 3)

Formulation	J_{ss} (mg·cm ⁻² ·h ⁻¹)	D (cm ² ·h ⁻¹)	P (cm·h ⁻¹)	T _{lag} (h)
Control	0.0093 $\pm$ 0.001	0.0236 $\pm$ 0.003	0.0314 $\pm$ 0.001	0.0836 $\pm$ 0.001
ME-CET-1	0.0325 $\pm$ 0.001	0.0673 $\pm$ 0.001	0.039 $\pm$ 0.001	0.056 $\pm$ 0.002
ME-CET-2	0.0257 $\pm$ 0.005	0.0402 $\pm$ 0.013	0.0308 $\pm$ 0.005	0.335 $\pm$ 0.011
ME-CET-3	0.0247 $\pm$ 0.002	0.1755 $\pm$ 0.018	0.029 $\pm$ 0.001	0.772 $\pm$ 0.082
ME-CET-4	0.0248 $\pm$ 0.001	0.1222 $\pm$ 0.011	0.029 $\pm$ 0.001	0.167 $\pm$ 0.138
ME-CET-5	0.0401 $\pm$ 0.004	0.124 $\pm$ 0.0108	0.048 $\pm$ 0.001	1.089 $\pm$ 0.094
ME-CET-6	0.0431 $\pm$ 0.003	0.112 $\pm$ 0.002	0.051 $\pm$ 0.001	1.201 $\pm$ 0.03
ME-CET-7	0.0391 $\pm$ 0.002	0.044 $\pm$ 0.0529	0.046 $\pm$ 0.001	1.96 $\pm$ 0.076
ME-CET-8	0.036 $\pm$ 0.001	0.135 $\pm$ 0.024	0.0432 $\pm$ 0.001	1.01 $\pm$ 0.186

**Figure 2.** Steady-state flux (J_{ss}) of cetirizine across rat skin (mean $\pm$ SD, n = 3). ME-CET-6 (highlighted) showed the highest flux.

sizes of 14.94 - 46.15 nm, with PDI < 0.5, indicate uniform nanoscale droplets suitable for skin delivery, consistent with previous systems from this group (23). The absence of phase separation and minimal changes in droplet size after 6 months support the physical stability of the optimized formulations.

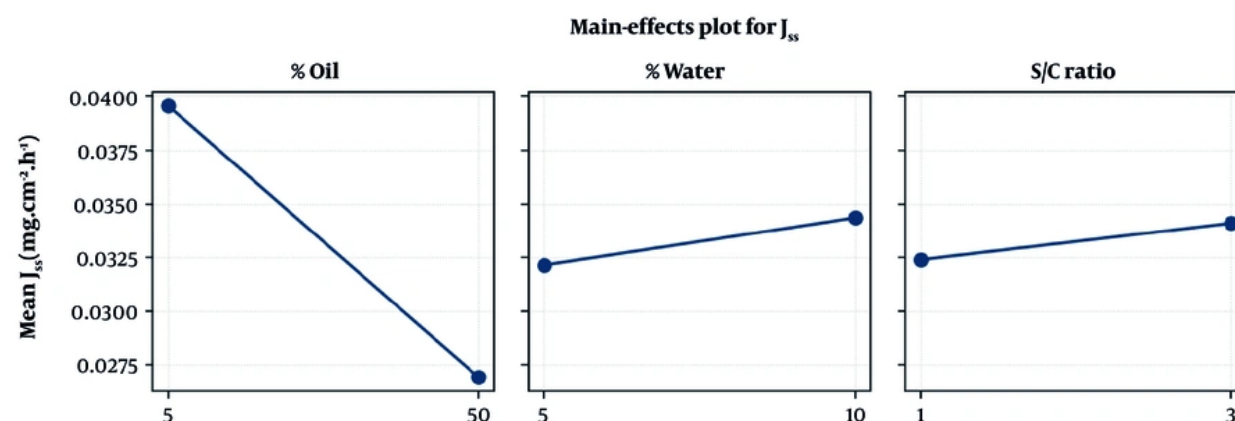
Viscosity increased with higher oil and lower water contents (both $P = 0.001$). pH values of 4.12 - 5.55 were related to water content ($P = 0.008$) and are compatible with topical use, although buffered adjustment toward the skin pH (~5.5) should be considered in future development.

Table 7. Corrected Enhancement Ratios for Flux (ERflux) and Diffusion (ERD = $D_{\text{form}}/D_{\text{control}}$) Relative to the Aqueous Control (Mean $\pm$ SD)

Formulation	ERflux	ERD (Corrected)
ME-CET-1	4.09 $\pm$ 0.14	2.85 $\pm$ 0.36
ME-CET-2	3.22 $\pm$ 0.45	1.70 $\pm$ 0.59
ME-CET-3	3.11 $\pm$ 0.11	7.44 $\pm$ 1.21
ME-CET-4	3.12 $\pm$ 0.15	5.18 $\pm$ 0.81
ME-CET-5	5.05 $\pm$ 0.15	5.25 $\pm$ 0.81
ME-CET-6	5.42 $\pm$ 0.12	4.75 $\pm$ 0.61
ME-CET-7	4.92 $\pm$ 0.06	1.86 $\pm$ 2.25
ME-CET-8	4.53 $\pm$ 0.19	5.72 $\pm$ 1.25

Table 8. Factorial ANOVA of Effects on Steady-State Flux (J_{ss})^a

Term	Coefficient	Effect	P value	Significance
Constant	0.0340	-	-	-
Oil (%)	-0.000281	-0.01264	0.001	Significant
Water (%)	+0.000440	+0.00220	0.119	NS
S/C ratio	+0.00185	+0.00370	0.015	Significant

^a Effect = coefficient $\times$ factor range.**Figure 3.** Main-effects plot for steady-state flux (J_{ss}): influence of oil content, water content, and S/C ratio.

ME-CET-6 achieved the highest flux (0.0431 $\text{mg}\cdot\text{cm}^{-2}\cdot\text{h}^{-1}$; ERflux, 5.42; $\sim 4.6\times$ control). Factorial ANOVA identified oil content as the dominant significant determinant ($P = 0.001$), with flux decreasing as oil content increased from 5% to 50%. The S/C ratio had a smaller but significant positive effect ($P = 0.015$), whereas water content was not significant. These findings indicate that, within the studied range, an

excessive oil phase may reduce drug thermodynamic activity or alter the microstructure in a way that limits release, whereas the lower-oil, lower-S/C formulation maintained a higher flux.

A key point concerns the mechanism. On re-examination, the diffusion enhancement ratio was recomputed consistently as $\text{ERD} = D_{\text{formulation}}/D_{\text{control}}$; the corrected values exceeded 1 for all formulations, reaching 7.44. Together with ERflux

Table 9. Comparison With Previous Cetirizine Transdermal/Topical Systems

System	Approach	Key outcome	Ref.
Present study	Microemulsion (oleic acid/Transcutol P), factorial	ERflux 5.42; ~4.6× vs control	-
Nanoemulsion gel	2 ³ factorial nanoemulsion gel; rat skin; clinical urticaria study	P = 7.65 cm·h ⁻¹ ; effective in urticaria	(36)
Enhancer study	Oleic acid/Tween 80/PG on cetirizine; DSC/FTIR	All enhancers raised permeability	(10)
Topical cetirizine	Solution, androgenetic alopecia (clinical)	Clinical topical efficacy	(9)

values > 3, these data suggest that both drug partitioning into the skin and apparent diffusivity were improved by the microemulsion system. Oleic acid can disrupt lipid packing in the stratum corneum, and Transcutol P may improve drug solubilization and skin partitioning; these mechanisms are consistent with the observed enhancement (18-21, 29).

From the measured flux, the translational potential can be estimated. At $J_{ss} = 0.0431 \text{ mg} \cdot \text{cm}^{-2} \cdot \text{h}^{-1}$, a patch of about 10 cm² would theoretically deliver ~10 mg/day, matching the oral therapeutic dose of 5 - 10 mg/day. Because excised rat skin overestimates human permeability, a conservative correction assuming human skin is ~9× less permeable still yields ~11.5 mg/day from a 100 cm² area, within the therapeutic range. These estimates are indicative only and require in vivo pharmacokinetic confirmation.

Zeta potential was not determined in this study. For nonionic surfactant microemulsions such as these, the absolute zeta potential is typically low; however, measurement is recommended for future characterization.

5.1. Study Limitations

This study was limited by ex vivo-only evaluation, the higher permeability of rat skin compared with human skin, the absence of pharmacokinetic and skin-irritation studies, the absence of direct mechanistic confirmation by DSC/FTIR in this work, and the lack of zeta-potential measurement. These limitations should be addressed before clinical translation.

5.2. Conclusions

Cetirizine microemulsions based on oleic acid and Transcutol P were formulated and optimized for transdermal delivery using a two-level full-factorial design. The formulations were nanoscale, uniform, and physically and chemically stable. ME-CET-6, containing 5% oil, 10% water, and an S/C ratio of 1:1, provided the highest ex vivo flux and permeability coefficient. Corrected enhancement ratios indicate that both

increased diffusivity and improved partitioning contributed to enhanced skin permeation. These findings support further development of cetirizine microemulsions for transdermal therapy, with in vivo pharmacokinetic, skin-irritation, and human-skin studies required for confirmation.

Footnotes

AI Use Disclosure: For the purpose of Text Editing, the An Ai Assistant (Claude) Was Used For Language Editing; All Scientific Content, Data, And Interpretations Are The Authors'. was used Moderate in the Introduction section.

Authors' Contribution: A. S., M. A. K., and H. H. K. conceived and designed the study. E. A. H. performed the formulation, characterization, release, and permeation experiments. A. S., M. A. K., H. H. K., and A. N. analyzed and interpreted the data. H. H. K., A. N., and Y. S. contributed to manuscript preparation and language editing. A. S. supervised the project and provided laboratory resources. All authors drafted and critically revised the manuscript, reviewed and approved the final version, and agreed to be accountable for all aspects of the work.

Conflict of Interests Statement: The authors do not declare any conflicts of interests for this study.

Data Availability: The data supporting the findings of this study are available from the corresponding author upon reasonable request.

Ethical Approval: All animal procedures were approved by the Animal Ethics Committee of Ahvaz Jundishapur University of Medical Sciences, Ahvaz, Iran (ethics code: IR.AJUMS.ABHC.REC.1402.075).

Funding/Support: This article was extracted from the Pharm.D. thesis of Ehsan Afshari Hoseinpur and was financially supported by the Vice-Chancellor for Research, Ahvaz Jundishapur University of Medical Sciences, Ahvaz, Iran (Project No. N-0222; webpage of the

grant:

<https://ethics.research.ac.ir/IR.AJUMS.ABHC.REC.1402.075>).

References

- Campoli-Richards DM, Buckley MMT, Fitton A. Cetirizine. A review of its pharmacological properties and clinical potential in allergic rhinitis, pollen-induced asthma, and chronic urticaria. *Drugs*. 1990;**40**(5):762-81. [PubMed ID: 1981354]. <https://doi.org/10.2165/00003495-199040050-00009>.
- Spencer CM, Faulds D, Peters DH. Cetirizine. A reappraisal of its pharmacological properties and therapeutic use in selected allergic disorders. *Drugs*. 1993;**46**(6):1055-80. [PubMed ID: 751061]. <https://doi.org/10.2165/00003495-199346060-00008>.
- Portnoy JM, Dinakar C. Review of cetirizine hydrochloride for the treatment of allergic disorders. *Expert Opin Pharmacother*. 2004;**5**(1):125-35. [PubMed ID: 14680442]. <https://doi.org/10.1517/14656566.5.1.125>.
- Walsh GM, Annunziato L, Frossard N, Knol K, Levander S, Nicolas JM, et al. New insights into the second generation antihistamines. *Drugs*. 2001;**61**(2):207-36. [PubMed ID: 11270939]. <https://doi.org/10.2165/00003495-200161020-00006>.
- Pagliara A, Testa B, Carrupt PA, Jolliet P, Morin C, Morin D, et al. Molecular properties and pharmacokinetic behavior of cetirizine, a zwitterionic H₁-receptor antagonist. *J Med Chem*. 1998;**41**(6):853-63. [PubMed ID: 9526560]. <https://doi.org/10.1021/jm970431i>.
- Chen C. Physicochemical, pharmacological and pharmacokinetic properties of the zwitterionic antihistamines cetirizine and levocetirizine. *Curr Med Chem*. 2008;**15**(21):2173-91. [PubMed ID: 18781943]. <https://doi.org/10.2174/092986708785747625>.
- Wang DY, Hanotte F, De Vos C, Clement P. Effect of cetirizine, levocetirizine, and dextrocetirizine on histamine-induced nasal response in healthy adult volunteers. *Allergy*. 2001;**56**(4):339-43. [PubMed ID: 11284803]. <https://doi.org/10.1034/j.1398-9995.2001.00775.x>.
- Simons FE, Simons KJ. Clinical pharmacology of new histamine H₁ receptor antagonists. *Clin Pharmacokinet*. 1999;**36**(5):329-52. [PubMed ID: 10384858]. <https://doi.org/10.2165/00003088-199936050-00003>.
- Seifian H, Safari Giv T, Abdollahimajd F, Namazi N. Topical cetirizine for the management of androgenic alopecia: results of a pilot study. *J Cosmet Dermatol*. 2024;**23**(2):708-10. [PubMed ID: 37697482]. <https://doi.org/10.1111/jocd.15989>.
- Soleymani SM, Mombeini R, Salimi A. Effect of various herbal and chemical enhancers on skin permeability to cetirizine: a study of changes in rat skin cells. *J Kerman Univ Med Sci*. 2024;**31**(3):126-34. <https://doi.org/10.34172/jkmu.2024.21>.
- Prausnitz MR, Langer R. Transdermal drug delivery. *Nat Biotechnol*. 2008;**26**(11):1261-8. [PubMed ID: 18997767]. [PubMed Central ID: PMC2700785]. <https://doi.org/10.1038/nbt.1504>.
- Barry BW. Novel mechanisms and devices to enable successful transdermal drug delivery. *Eur J Pharm Sci*. 2001;**14**(2):101-14. [PubMed ID: 11500256]. [https://doi.org/10.1016/S0928-0987\(01\)00167-1](https://doi.org/10.1016/S0928-0987(01)00167-1).
- Naik A, Kalia YN, Guy RH. Transdermal drug delivery: overcoming the skin's barrier function. *Pharm Sci Technol Today*. 2000;**3**(9):318-26. [PubMed ID: 10996573]. [https://doi.org/10.1016/S1461-5347\(00\)00295-9](https://doi.org/10.1016/S1461-5347(00)00295-9).
- Lawrence MJ, Rees GD. Microemulsion-based media as novel drug delivery systems. *Adv Drug Deliv Rev*. 2000;**45**(1):89-121. [PubMed ID: 1104900]. [https://doi.org/10.1016/S0169-409X\(00\)00103-4](https://doi.org/10.1016/S0169-409X(00)00103-4).
- Kreilgaard M. Influence of microemulsions on cutaneous drug delivery. *Adv Drug Deliv Rev*. 2002;**54**:S77-S98. [PubMed ID: 12460717]. [https://doi.org/10.1016/S0169-409X\(02\)00116-3](https://doi.org/10.1016/S0169-409X(02)00116-3).
- Kogan A, Garti N. Microemulsions as transdermal drug delivery vehicles. *Adv Colloid Interface Sci*. 2006;**123** - **126**:369-85. [PubMed ID: 16843424]. <https://doi.org/10.1016/j.cis.2006.05.014>.
- Heuschkel S, Goebel A, Neubert RHH. Microemulsions - modern colloidal carrier for dermal and transdermal drug delivery. *J Pharm Sci*. 2008;**97**(2):603-31. [PubMed ID: 17696162]. <https://doi.org/10.1002/jps.20995>.
- Williams AC, Barry BW. Penetration enhancers. *Adv Drug Deliv Rev*. 2004;**56**(5):603-18. [PubMed ID: 15019749]. <https://doi.org/10.1016/j.addr.2003.10.025>.
- Naik A, Pechtold LARM, Potts RO, Guy RH. Mechanism of oleic acid-induced skin penetration enhancement in vivo in humans. *J Control Release*. 1995;**37**(3):299-306. [https://doi.org/10.1016/0168-3659\(95\)00088-7](https://doi.org/10.1016/0168-3659(95)00088-7).
- Sintov AC, Shapiro L. New microemulsion vehicle facilitates percutaneous penetration in vitro and cutaneous drug bioavailability in vivo. *J Control Release*. 2004;**95**(2):173-83. [PubMed ID: 14980766]. <https://doi.org/10.1016/j.jconrel.2003.11.004>.
- Osborne DW, Musakhanian J. Skin penetration and permeation properties of Transcutol - neat or diluted mixtures. *AAPS PharmSciTech*. 2018;**19**(8):3512-33. [PubMed ID: 30421383]. [PubMed Central ID: PMC6848246]. <https://doi.org/10.1208/s12249-018-1196-8>.
- Moghimpour E, Salimi A, Eftekhari S. Design and characterization of microemulsion systems for naproxen. *Adv Pharm Bull*. 2013;**3**(1):63-71. [PubMed ID: 24312814]. [PubMed Central ID: PMC3846048]. <https://doi.org/10.5681/apb.2013.011>.
- Jamali N, Moghimipour E, Hedayatipour N, Salimi A. Preparation, characterization, and skin permeation evaluation of naproxen microemulsions for transdermal delivery. *Jundishapur J Nat Pharm Prod*. 2024;**19**(3). e145137. <https://doi.org/10.5812/jjnpp-145137>.
- Heidari Kaydan H, Sharif makhmlzadeh B, Feghihi M, Rezaei A, Bagheri F, Salimi A. Preparation and characterization of ozonated liposomes loaded with curcumin: a potential approach for diabetic retinopathy treatment. *Jundishapur J Nat Pharm Prod*. 2024;**19**(4). e153745. <https://doi.org/10.5812/jjnpp-153745>.
- Kaydan HH, Moghimipour E, Dalvand H, Jamali N, Salimi A, Salimi A. Design, preparation, and ex vivo skin permeation of doxepin microemulsion system for topical delivery. *J Cosmet Dermatol*. 2025;**24**(1). e16786. [PubMed ID: 39838580]. [PubMed Central ID: PMC11751381]. <https://doi.org/10.1111/jocd.16786>.
- Javadiyeh A, Heidari Kaydan H, Bagheri F, Goodarzi S, Salimi A. Design, preparation, and ex vivo skin permeation of naringenin liposomal formulation for topical delivery. *Jundishapur J Nat Pharm Prod*. 2026;**21**(1). e168429. <https://doi.org/10.5812/jjnpp-168429>.
- Higuchi T. Mechanism of sustained-action medication. Theoretical analysis of rate of release of solid drugs dispersed in solid matrices. *J Pharm Sci*. 1963;**52**(12):1145-9. [PubMed ID: 14088963]. <https://doi.org/10.1002/jps.2600521210>.
- Korsmeyer RW, Gurny R, Doelker E, Buri P, Peppas NA. Mechanisms of solute release from porous hydrophilic polymers. *Int J Pharm*. 1983;**15**(1):25-35. [https://doi.org/10.1016/0378-5173\(83\)90064-9](https://doi.org/10.1016/0378-5173(83)90064-9).
- Barry BW. Lipid-protein-partitioning theory of skin penetration enhancement. *J Control Release*. 1991;**15**(3):237-48. [https://doi.org/10.1016/0168-3659\(91\)90115-T](https://doi.org/10.1016/0168-3659(91)90115-T).
- Percie du Sert N, Hurst V, Ahluwalia A, Alam S, Avey MT, Baker M, et al. The ARRIVE guidelines 2.0: updated guidelines for reporting animal research. *PLoS Biol*. 2020;**18**(7). e3000410. [PubMed ID: 32663219]. [PubMed Central ID: PMC7360023]. <https://doi.org/10.1371/journal.pbio.3000410>.
- Jamali N, Moghimipour E, Nikpour F, Salimi A. Development and ex-vivo skin permeation of sildenafil citrate microemulsion system for transdermal delivery. *Iran J Pharm Res*. 2024;**23**(1). e139381. [PubMed

- ID: [39140102](#)]. [PubMed Central ID: [PMC11319783](#)]. <https://doi.org/10.5812/ijpr-139381>.
32. Salimi A, Hoseinzadeh H, Mohammad Soleymani S. Development and optimization of a methimazole microemulsion for topical application: formulation characteristics and transdermal permeation. *J Cosmet Dermatol*. 2024;**23**(12):4315-24. [PubMed ID: [39135289](#)]. [PubMed Central ID: [PMC11626322](#)]. <https://doi.org/10.1111/jocd.16528>.
 33. Salimi A, Jafarian S, Salimi A, Mohammad Soleymani S. Formulation and evaluation of valproic acid microemulsions for enhanced transfollicular delivery in guinea pig skin. *J Cosmet Dermatol*. 2025;**24**(2). e16685. [PubMed ID: [39563603](#)]. [PubMed Central ID: [PMC11845931](#)]. <https://doi.org/10.1111/jocd.16685>.
 34. Moghimipour E, Farsimadan N, Salimi A. Ocular delivery of quercetin using microemulsion system: design, characterization, and ex-vivo transcorneal permeation. *Iran J Pharm Res*. 2022;**21**(1). e127486. [PubMed ID: [36945341](#)]. [PubMed Central ID: [PMC10024810](#)]. <https://doi.org/10.5812/ijpr-127486>.
 35. Sajadi Bami M, Fakhraei Lahij S, Mobedi H, Hamidi M, Vahidi R, Khazaeli P. Development and optimization of dissolvable polymeric microneedle patch for transdermal delivery of lawsone. *Jundishapur J Nat Pharm Prod*. 2026;**21**(1). e169497. <https://doi.org/10.5812/jjnpp-169497>.
 36. Kassem MA, Ghalwash MM, Abdou EM. Development of nanoemulsion gel drug delivery systems of cetirizine; factorial optimisation of composition, in vitro evaluation and clinical study. *J Microencapsul*. 2020;**37**(6):413-30. [PubMed ID: [32421463](#)]. <https://doi.org/10.1080/02652048.2020.1771446>.